

## Full Length Articles

# Striatal topography of probability and magnitude information for decisions under uncertainty

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## ABSTRACT

Most decisions involve some element of uncertainty. When the outcomes of these decisions have different likelihoods of occurrence, the decision-maker must consider both the magnitude of each outcome and the probability of its occurrence, but how do individual decision makers combine the two dimensions of magnitude and probability? Here, we approach the problem by separating in time the presentation of magnitude and probability information, and focus the analysis of fMRI activations on the first piece of information only. Thus, we are able to identify distinct neural circuits for the two dimensions without the confounding effect of divided attention or the cognitive operation of combining them. We find that magnitude information correlates with the size of the response of the ventral striatum while probability information correlates with the response in the dorsal striatum. The relative responsiveness of these two striatal regions correlates with the behavioral tendency to weight one more than the other. The results are consistent with a second-order process of information aggregation in which individuals make separate judgments for magnitude and probability and then integrate those judgments.

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## Introduction

Most decisions involve some element of uncertainty. When the outcomes of these decisions have different likelihoods of occurrence, the decision-maker must consider both the magnitude of each outcome and the probability of its occurrence. In traditional economic analysis, individuals are assumed to make decisions to maximize their *expected utility*, where the expected utility is the benefit of each possible outcome multiplied by the probability of its occurrence (von Neumann and Morgenstern, 1944). Variations of expected utility theory (EUT) allow for distortions of the utility and probability functions (Allais, 1953; Kahneman and Tversky, 1979; Starmer, 2000). For outcomes with positive utility, all current models of rational choice require the monotonic combination of probability with expected utility. In other words, larger magnitudes of outcomes are better than smaller ones, and higher probabilities are better than lower ones.

How do individual decision makers combine the two dimensions of magnitude and probability? The single system hypothesis suggests that a combined metric of expected utility, including both probability and magnitude, exists throughout brain systems that play a role in decision making but particularly in reward-related regions like striatum and perceptual decision regions like parietal cortex (Fiorillo et al., 2003; Glimcher et al., 2005; Kable and Glimcher, 2007). In contrast, the dual system hypothesis suggests that there are largely distinct neural

systems for the processing of magnitude and probability. While reward-related brain regions, particularly the ventral striatum, are consistently found to have increased activity in response to higher magnitudes of expected reward (Knutson et al., 2001; Tobler et al., 2005; Tom et al., 2007; Yacubian et al., 2006), a variety of different regions have been observed to encode variables related to probability of reward, including insula, ventromedial prefrontal cortex (VMPFC), dorsolateral prefrontal cortex (DLPFC), anterior cingulate cortex (ACC), and parietal cortex (Berns et al., 2008; Hsu et al., 2005; Huettel et al., 2006; Knutson et al., 2005; Paulus et al., 2001; Platt and Glimcher, 1999; Shadlen and Newsome, 2001; Venkatraman et al., 2009).

It has been surprisingly difficult to reach consensus about the separability of probability weighting, utility, and expected utility in the brain. Many of the human studies suggest that these elements are separable, but many of the non-human primate studies suggest that they are not. Undoubtedly, much of the disagreement arises from differences in the way in which experiments are operationalized, differences in how monkeys and humans learn, and differences between experiential learning (e.g. reinforcement learning) versus cognitive learning (e.g. learning to multiply two numbers together). Part of the problem is that when making risky decisions, agents are presented with two dimensions of information. It has been demonstrated that when individuals are faced with multiple dimensions of information, they tend to make judgments on each dimension and then integrate the judgments, as opposed to integrating the information and then making a judgment (Shaw, 1982). Here, we approach the problem by separating in time the presentation of magnitude and probability information, and focus the analysis of fMRI activations on the

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first piece of information only. This approach isolates the processing of magnitude and probability without the confounding effect of divided attention or the cognitive operation of combining them.

## Methods and materials

### Participants

Thirty participants (21 female, 9 male; 18–45 years) were recruited from the Emory University campus area. All participants were right-handed, reported no psychiatric or neurological disorders, or other characteristics that might preclude them from safely undergoing MRI. All participants provided informed consent to experimental procedures approved by the Emory University Institutional Review Board. Participants received a base pay of \$40 with the opportunity to win an additional \$80 depending on decisions made during the experiment.

### Task design

The experimental task was designed to measure independently the neural responses to two dimensions of a simple lottery decision: the probability of an outcome and the magnitude of the outcome. While previous studies have presented both pieces of information simultaneously, it is generally impossible to know how an individual allocates their attention to probability and magnitude. Here, we measured responses to probability and magnitude by separating the delivery of the two pieces of information by presenting only one piece at a time (Fig. 1).

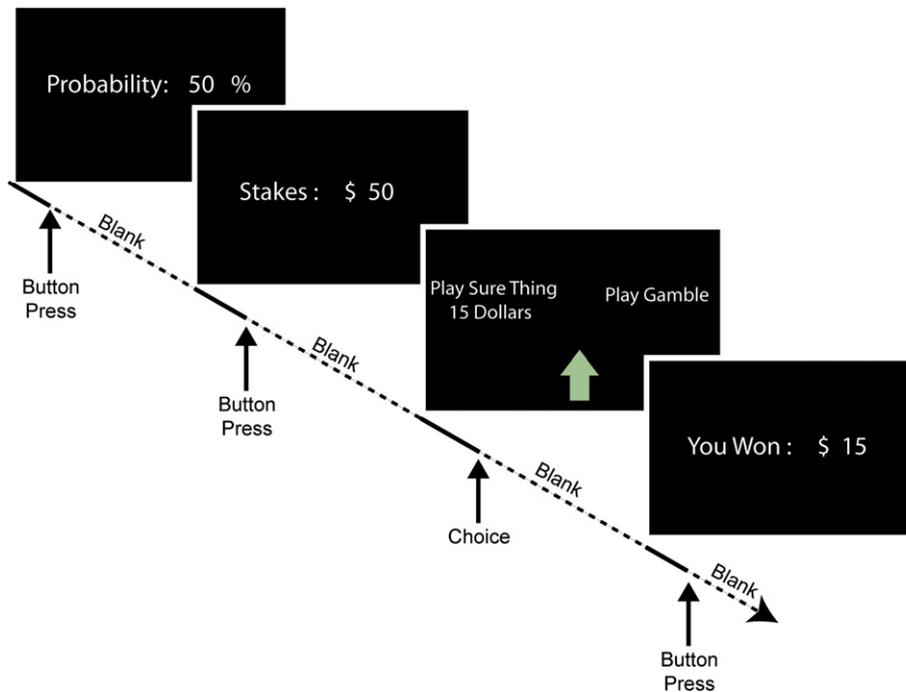
We used five different values for both the magnitudes and probabilities: 20, 30, 50, 70, and 80. Magnitude was denoted by \$ (e.g. \$ 20), and probability was denoted by % (e.g. 20%). A trial consisted of the display of both magnitude and probability information, but three different order conditions were used: 1) probability then magnitude (each presented alone), 2) magnitude then probability (each presented alone), and 3) probability and magnitude simultaneously. The third condition was divided so that half of these trials presented

the probability on top and the other half presented the magnitude on top. With five values for both probability and magnitude, there were 25 combinations, and each was presented in each of the three order conditions, for a total of 75 trials. These trials were divided into 4 runs of approximately 19 trials each, which lasted approximately 10 min, depending on individuals' decision times. On each trial, the participant had to choose either the lottery or the default "sure thing" option of \$15, which was equivalent to the average expected value of all of the lotteries. Participants indicated their decision between "The Sure Thing of \$15" and "Play Gamble" by moving an arrow to point at their choice. After their choice, the outcome was displayed. To calculate the outcome for each accepted gamble, an integer between 1 and 100 was randomly chosen. If the random number was less than the trial probability, then the participant won the stakes from the trial. The outcome was always presented even when the participant chose the sure thing. After completion of all four runs and all scans, the participant rolled a dice to randomly choose one trial to realize their winnings.

The order of the trials was predetermined by a random number generator and was identical for every participant. Each of the 75 trials had the same layout, differing only by the order of the information presented in each trial. All of the inter-stimulus intervals (ISI) and inter-trial intervals (ITI) were jittered and optimized prior to the start of the experiment and were predetermined and identical for all participants.

### MRI scanning

Neuroimaging data were collected using a 3 Tesla Siemens Magnetom Trio whole body scanner (Siemens Medical Systems, Erlangen, Germany). Functional data consisted of thirty-three axial slices that were sampled with a thickness of 3.5 mm and encompassing a field of view of 192 mm with an inplane resolution of  $64 \times 64$  (T2\* weighted, TR = 2000 ms, TE = 30 ms). fMRI data were analyzed using SPM5 (Wellcome Department of Imaging Neuroscience, University College London) using a standard 2-stage random-effects regression model.



**Fig. 1.** Timeline of a trial in which probability and magnitude information are separated in time. This is an example of a "Probability First" trial. The probability of winning is shown first (minimum of 2 s up to a button press), which is followed by a variable length blank screen. The magnitude of the stakes is then shown similarly, which is followed by the choice screen, and then the results of the choice. All blank screen durations were variable from 2 to 6 s. "Magnitude first" trials reversed the order of stakes magnitude and probability information. "Simultaneous" trials presented both probability and magnitude on one screen.

Data were subjected to standard preprocessing, including motion correction, slice timing correction, normalization to an MNI template brain and smoothing using an isotropic Gaussian kernel (full-width half-maximum = 8 mm).

### Behavioral model

We formulated a behavioral model to see how the different conditions influenced the participants' decisions. By design, the experiment separately presented probability and magnitude, so the initial behavioral models included independent and additive terms for probability and magnitude. For each individual subject, we used logistic regression to determine the weight of the following factors on the likelihood of accepting the gamble: probability, stakes, and order:

$$\log \left[ \frac{PG_i}{(1-PG_i)} \right] = \beta_0 + \beta_{prob} Probability_i + \beta_{mag} Magnitude_i + \beta_{P1st} ProbFirst_i + \beta_{M1st} MagFirst_i \quad (1)$$

where, on trial  $i$ ,  $PG$  is the likelihood of accepting the gamble,  $Probability$  is the probability (20%, 30%, 50%, 70%, 80%),  $Magnitude$  is the outcome (\$20, \$30, \$50, \$70, \$80), and  $ProbFirst$  and  $MagFirst$  are dummy variables for the condition order (0 & 0 is the simultaneous condition).

The results of this analysis showed that the coefficients for order were not significant in any subject. Subsequently, we used a reduced model with only probability and magnitude:

$$\log \left[ \frac{PG_i}{(1-PG_i)} \right] = \beta_0 + \beta_{prob} Probability_i + \beta_{mag} Magnitude_i \quad (2)$$

In this model, all coefficients were significant for all participants except three people, who were excluded from subsequent analyses. From this model, we calculated a subjectwise parameter that gauged the relative sensitivity to probability and magnitude:  $PM_{diff} = \beta_{prob} - \beta_{mag}$ .

Although this additive model was well-suited for the serial design of the experiment, it makes stronger assumptions than a standard expected utility (EU) model (in particular, linearity and additivity). For comparison to forms that assume maximization EU, we also fit the following two behavioral models:

$$\log \left[ \frac{PG_i}{(1-PG_i)} \right] = \beta_0 + \beta_{prob} Probability_i + \beta_{mag} Magnitude_i + \beta_{EV} Prob_i Mag_i \quad (3)$$

which allowed for the multiplicative interaction of probability and magnitude, and more conventionally an EU-type model:

$$\log \left[ \frac{PG_i}{(1-PG_i)} \right] = \beta_0 + \beta_{EV} Prob_i Mag_i^\alpha \quad (4)$$

where  $\alpha$  was varied from 0.2 to 1.5 with the best fit for each subject determined by Akaike's information criterion (AIC).

### fMRI analysis

To minimize the effects of automatization (making the same responses to probability and magnitude combinations without thinking about it), we focused our analysis on the initial presentations of each combination and thus restricted the fMRI analysis to the first two runs (Phelps et al., 2001). At the first level, the model contained seven conditions. The first five conditions indicated the type of information and the order in which it was presented: probability first, magnitude first, probability second, magnitude second, and both simultaneously. Each of these conditions was modeled as a variable duration event for the time that the information was presented. Probability and magnitude were included as parametric modulators for

their corresponding conditions. The sixth and seventh conditions segregated the choice period into "sure thing" and "gamble" trials (also variable duration events up to, and including, the choice). Subject motion parameters were included as nuisance regressors. All regressors were convolved with a standard HRF function. Contrasts from the first-level model were entered into a second-level model using a one-sample t-test. Using the AlphaSim routine in AFNI, we estimated the combination of height and extent thresholds that yielded a whole-brain FDR < 0.05 (10,000 iterations). We used 3dFWHMx to estimate the image smoothness from the square root of the SPM-generated ResMS image and input into AlphaSim. Finally, using a voxel level threshold of  $P < 0.001$ , the extent threshold that yielded a cluster level alpha of 0.05 was determined to be  $k \geq 49$  (Logan and Rowe, 2004; Zhang et al., 2009).

To identify probability-responsive regions and magnitude-responsive regions, we examined the contrasts formed from the parametric modulators for probability and magnitude on the probability-first and magnitude-first conditions respectively. Because only one piece of information had been presented at that point in the trial, this approach eliminates the possibility of divided attention between two pieces of information. Beta values from these contrasts were then extracted from regions of interest (primarily the striatum) and checked for correlation with the  $PM_{diff}$  metric for each subject.

### Results

The behavioral model indicated that probability and magnitude were both positively correlated with the likelihood of accepting the gamble over the sure thing. Except for three subjects, the coefficients for probability and magnitude (Eq. (2)) were significant for all participants (see supplement). Consequently, the form with an interaction term in Eq. (3) was overspecified and resulted in almost no significant coefficients. The form based on an EU-type function (Eq. (4)) yielded significant coefficients for all subjects. However, when we compared the fit of Eqs. (2) and (4), the models were not significantly different based on the AIC [paired  $T(29) = 1.41$ ,  $p = 0.170$ ]. The average  $r^2$  for both models was essentially the same (0.66 for EU and 0.64 for additive) and not significantly different [paired  $T(29) = 1.77$ ,  $p = 0.09$ ]. Thus, we conclude that the additive model is as good (or no worse) than an EU-type model, but the additive model has the advantage of separating the weighting of probability and magnitude. There was substantial variation in the size of the coefficients and the difference between  $\beta_{prob}$  and  $\beta_{mag}$ . The mean  $PM_{diff}$  was 5.835 (7.09 s.d.). Thus, for most subjects  $\beta_{prob}$  was greater than  $\beta_{mag}$ , indicating that probability had a greater effect on their decision than magnitude. The consistency of subjects' choices was measured by the percentage of times a given combination of probability and magnitude resulted in the same choice (gamble or sure thing). On average, subjects made the same choice 78% of the time (range: 60–100%).

Analysis of decision times indicated that subjects got steadily faster in each run, from an average of 724 ms in run 1 to 610 ms in run 4 [ $F(3,87) = 6.25$ ,  $P < 0.001$ ]. The decision times in run 1 and 2 were not significantly different from each other [ $F(1,29) = 1.29$ ,  $P = 0.266$ ], the difference between run 1 and 3 trended toward significance [ $F(1,29) = 3.43$ ,  $P = 0.074$ ], and the difference between run 1 and 4 were significantly different [ $F(1,29) = 16.1$ ,  $P < 0.001$ ], thus supporting the combination of fMRI runs 1 and 2 in the analysis, and separating out runs 3 and 4.

Several brain regions showed correlations with probability or magnitude when those pieces of information were presented first (Table 1). The striatum, however, was of particular interest. We found that both probability and magnitude were correlated with striatal activity, but there was a clear topography with the dorsal striatum correlated with probability and the ventral striatum correlated with magnitude (Fig. 2). To determine whether these apparent differences in topography were

**Table 1**

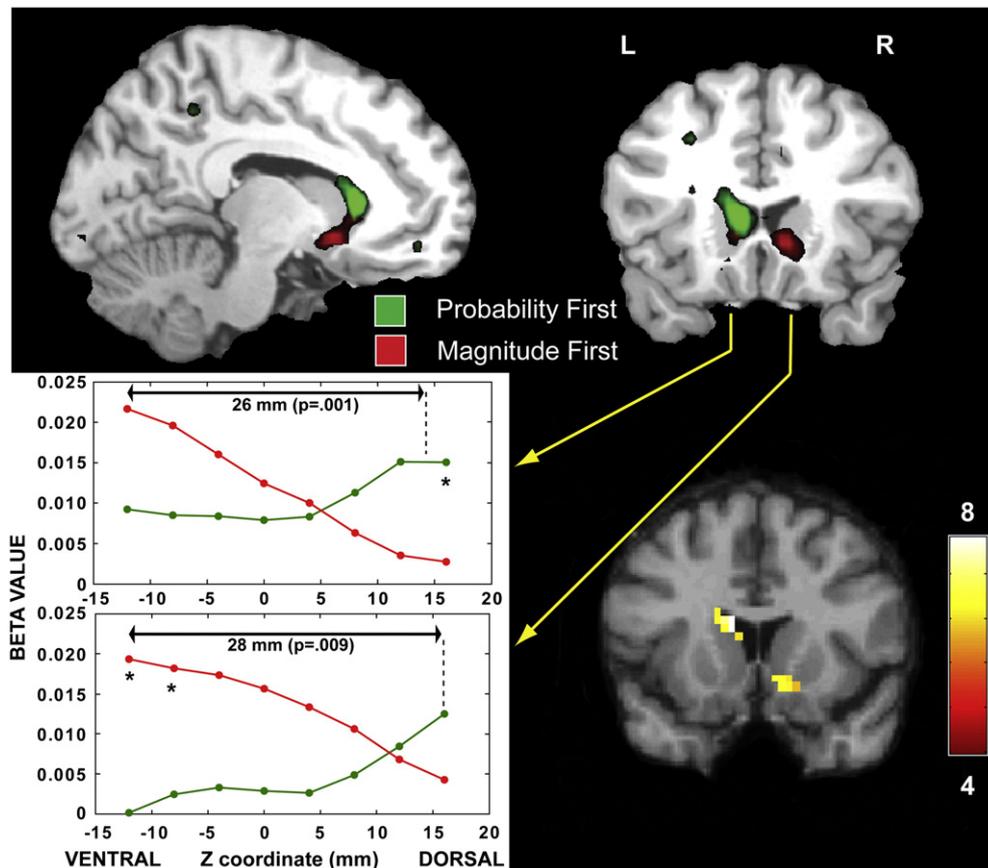
Brain regions correlated with parametric modulators for probability and magnitude. Regions were thresholded at voxel level  $P < 0.001$  and cluster size  $\geq 49$ . The subjectwise correlation ( $R$ ) with measures of probability-magnitude weighting ( $PM_{diff}$ ) are shown (and significance,  $P$ ).

Region	MNI coordinates	Voxels	Z	R with $PM_{diff}$	P
<b>Probability first</b>					
Dorsal striatum	-9, 21, 7	85	4.97	0.02	0.93
Visual cortex	30, -78, 14	284	4.45	-0.09	0.65
Parahippocampal gyrus	24, -27, -7	110	4.04	-0.135	0.5
<b>Magnitude first</b>					
Ventral striatum	6, 3, -11	229	4.37	-0.5	0.008
Posterior cingulate cortex	18, -36, 35	60	4.24	-0.32	0.11
L DLPFC	-24, 30, 11	71	3.73	-0.26	0.19
Thalamus	-3, -15, 11	50	3.65	-0.34	0.08

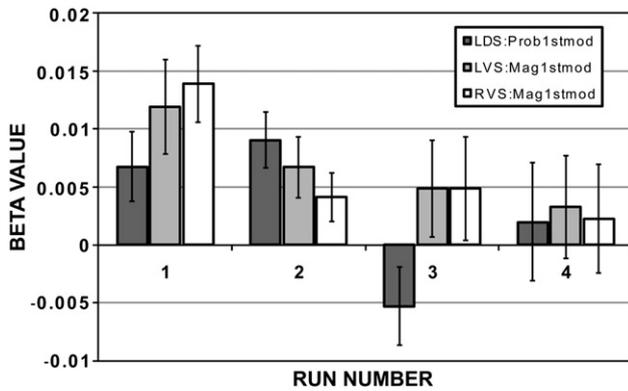
statistically different, we took two approaches. First, we examined the contrast between prob1st (modulated by probability) and mag1st (modulated by magnitude). We restricted this analysis to the striatal regions identified in the corresponding individual contrasts by using them as a masking. Within these regions, the dorsal and ventral extremes were significantly different on a voxelwise basis ( $P < 0.05$ , implementing a two-sided t-test via an F-contrast in SPM). Second, because the two regions of the striatum are in close proximity, the spatial smoothing performed in the preprocessing would be expected to result in the overlap of two gaussians. This was confirmed by examining a cross-section of beta values as a function of the Z-coordinate through the head of the caudate

(Fig. 2). Here, we find evidence of opposing gradients along the ventral-dorsal axis for probability and magnitude information, which was significantly different on a voxelwise basis at the extremes. Moreover, from these cross-sections, we can estimate a distance of approximately 26–28 mm between the spatial peaks of the probability and magnitude information. Given the spatial width of these profiles, we determined whether the distance between the peaks was significantly different. A Z-statistic was calculated by:  $Z = d / \sqrt{(\sigma_1^2/2 + \sigma_2^2/2)}$  where  $d$  is the distance between the peaks and  $\sigma_1$  and  $\sigma_2$  are the standard deviations of the two spatial profiles. With this method, the centroids of probability and magnitude information were statistically different in both the left ( $Z = 3.30, P = 0.001$ ) and right striatum ( $Z = 2.62, P = 0.009$ ).

When the beta values for the parametric modulators of probability and magnitude were extracted from these ROIs for each run separately, we found a declining trend such that all were essentially zero by the fourth run (Fig. 3). Given that the behavioral choices were not significantly different across runs, this suggests some form of neural habituation and the rationale for using the initial presentations in the first 2 runs as the best estimate of neural responsiveness to probability and magnitude information. Extracting the beta values for the parametric modulators of probability1st x probability and magnitude1st x magnitude for the magnitude-first and probability-first regions in Fig. 2, and averaging over the voxels within each region, we found a significant negative correlation of  $PM_{diff}$  with the betas for magnitude in the ventral striatum (Fig. 4) but no correlation with  $PM_{diff}$  with the betas for probability in the dorsal striatum ( $R = 0.02, p = 0.93$ ). Importantly, since the regions were defined by the parametric modulators for



**Fig. 2.** Brain regions in which the BOLD activation was correlated with the probability (green) or magnitude (red) of the outcome when presented as the first piece of information ( $P < 0.001$ ). The level of striatal response was correlated with both probability and magnitude but was topographically distinct with probability located dorsally and magnitude ventrally. The spatial profile of activation (lower left) for the left (upper panel) and right (lower panel) striatum indicated opposing gradients along the ventral-dorsal axis (X coordinate =  $\pm 12$ , Y coordinate = 16). From these cross-sections, we estimate a distance of approximately 26–28 mm between the spatial peaks of the probability and magnitude information. Given the spatial width of these profiles, the distance between the peaks was significantly different in both the left ( $Z = 3.30, P = 0.001$ ) and right striatum ( $Z = 2.62, P = 0.009$ ). This was confirmed on a voxelwise basis ( $*P < 0.05$ ) within the striatal clusters by an F-test on the contrast of parametric modulators: [prob1st x prob – mag1st x mag] (lower right), which was masked by the union of the probability and magnitude contrasts above [ $F(1,28) > 4, P < 0.05$ ].



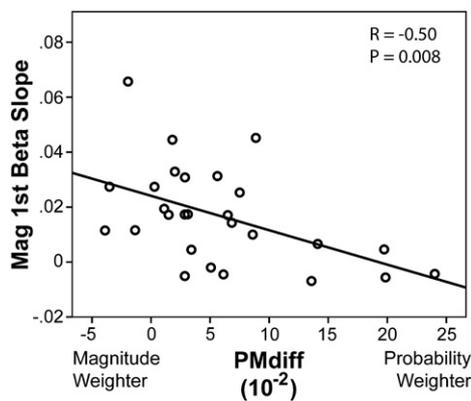
**Fig. 3.** Beta values within the left (LVS) and right (RVS) ventral striatum and left dorsal striatum (LDS) ROIs as a function of run number. The beta values for the parametric modulators of probability 1st x probability and magnitude 1st x magnitude were averaged within the ROIs shown in Fig. 2 separately for each run. All regions showed a declining trend in the size of the beta values as run number increased, such that they were all essentially zero by run 4. Given that behavioral choices were unchanged with run number, this suggests a neural habituation with repetition.

probability and magnitude across all subjects (without regard to the  $PM_{diff}$  metric), the correlation to  $PM_{diff}$  is independent of the identification of the ROIs (Vul et al., 2009).

## Discussion

It has long been known that individuals do not combine probability information in a linear manner with magnitude information. Prospect theory, and subsequent variants, have proposed a nonlinear weighting function in which low probabilities are overestimated and high probabilities underestimated (Kahneman and Tversky, 1979; Prelec, 1998; Tversky and Kahneman, 1992; Wu and Gonzalez, 1996). Although these S-shaped forms fit aggregate data, there is a high degree of subject heterogeneity (Abdellaoui, 2000). Moreover, few mechanistic explanations exist for the underlying cause of these distortions.

Previous neuroeconomic experiments of decision making under uncertainty have typically presented both elements simultaneously (Berns et al., 2008; Christopoulos et al., 2009; Hsu et al., 2009; Huettel et al., 2006; Smith et al., 2009). The implicit assumption has been that people do, in fact, consistently combine probability and magnitude information. However, a large body of research has shown that when multiple pieces of information are presented simultaneously, individuals naturally focus their attention on some elements more than others.



**Fig. 4.** Relationship between the relative degree that individuals weighted probability and magnitude information in their decisions ( $PM_{diff}$ ) to the degree of activation in the ventral striatum to magnitude information (Mag 1st Beta Slope). The slope of the activation is a measure of how much the BOLD signal increases per dollar of the outcome. Subjects who were strong magnitude weighters (left) had significantly more responsiveness to magnitude information in the ventral striatum than probability weighters (right).

Thus, the problem with presenting probability and magnitude simultaneously is that in most neuroimaging experiments we don't know how an individual is dividing their attention. Consequently, a failure to observe responses in a particular brain region may not mean that the region doesn't process a type of information; it could also be the case that nobody paid attention to it. Here, we address this limitation by presenting probability and magnitude information separately. Although one might argue that this is an artificial separation, even when the two pieces of information are presented simultaneously, the subject still must read them sequentially. Our design simply controls this process and extends it in time.

The finding that the ventral striatum processes expected magnitude is consistent with a large body of research that has demonstrated this structure's role in processing the expectation of reward. In this context, it is not surprising that the ventral striatum activity correlated with the magnitude of the expected payoff. Signals in the ventral striatum have been variously interpreted as reward expectation (Knutson et al., 2001; Knutson et al., 2005), reward prediction error (Montague and Berns, 2002; O'Doherty et al., 2004; Samejima et al., 2005; Schultz and Dickinson, 2000; Schultz et al., 1997), incentive salience (Robinson and Berridge, 1993; Zink et al., 2004), and expected utility (Glimcher et al., 2005; Rangel et al., 2008). What is common across all of these interpretations, however, is the monotonic relationship between the magnitude of the reward and the magnitude of the response in the ventral striatum. The larger the expected reward (or RPE), the larger the striatal response. Our findings are consistent with this monotonicity.

While the ventral striatum was linked to magnitude information, we found that the dorsal striatum was correlated with probability information. Although several studies have demonstrated probability-related signals in the striatum for passive tasks (Delgado et al., 2005; Knutson et al., 2005; Preuschoff et al., 2006; Tobler et al., 2007; Yacubian et al., 2006), relatively few have directly varied probability with the goal of identifying probability-specific signals in the brain during choice. Three previous studies of choice examined brain regions correlated with the probability of monetary outcome, with one identifying the striatum (Hsu et al., 2009) and two not (Paulus and Frank, 2006; Smith et al., 2009). Interestingly, Hsu et al. identified a region of the striatum intermediate between the ventral and dorsal zones that we found associated with magnitude and probability respectively. Similarly, in a previous study of choice for probabilistic electric shocks, we also found evidence for the encoding of probability in the dorsal striatum (Berns et al., 2008). However, all of these experiments presented probability and magnitude information simultaneously.

Although we found differences in the striatal location between magnitude and probability processing, these differences were subtle. When considered in isolation, the individual contrasts of magnitude and probability information were indicative of ventral and dorsal locations. The arbitrary nature of thresholding, however, might give the appearance of two regions being distinct. As an alternative test, we considered the voxelwise difference between magnitude and probability contrasts. This revealed two clusters within the union of the two contrasts, but at modest significance levels (ranging from  $P=0.05$  to  $0.01$ ). These two clusters were located at the dorsal and ventral extremes of the striatum (Fig. 2). However, a voxelwise comparison has limited power when two regions of activation lie in such close proximity to each other. Because the striatum is a small structure, and the activation data were smoothed with a gaussian kernel, it is possible that even if magnitude and probability information were processed in distinct striatal regions, we might not detect them due to smoothing. A more appropriate test of separation should consider the spatial profile of activation. In fact, when plotted in cross-section along the ventral-dorsal axis, we found a gaussian profile of activation for both magnitude and probability information on both the left and right (Fig. 2). When the distance between the peaks of these profiles was compared to their widths with a Z-test,

we found that the locations of magnitude and probability information were significantly different ( $P=0.001$  and  $.009$  for left and right sides). Although the Z-test in space is strongly indicative of separate striatal locations for magnitude and probability, we note that there is still a large degree of overlap in the middle striatum, suggesting a possible location in which the two dimensions are combined during decision making.

Several previous studies have implicated the dorsal striatum in aspects of decision making, particularly reinforcement learning (Jessup and O'Doherty, 2011; Li and Daw, 2011; O'Doherty et al., 2004; Samejima et al., 2005). While the role of the striatum, particularly the ventral striatum, is well established in classical conditioning and signaling reward-prediction errors, there is less agreement when it comes to decision-making tasks and instrumental learning. With more sophisticated models that include choice policies, the specific role of the dorsal striatum has been suggested to function as the "actor" in actor-critic models (Li and Daw, 2011; O'Doherty et al., 2004). In these models, the actor uses a prediction-error signal to modify the associations between stimuli and responses. However, as Li and Daw noted, the dissociation of value and policy signals has been difficult in choice tasks due to the conflation of value and choice in most experimental designs (Li and Daw, 2011). Thus, the issue of whether the dorsal striatum is primarily involved in mapping stimulus-response relationships or signaling reward prediction errors of outcomes is still debated (Balleine et al., 2007).

Although there are commonalities of our experiment with the RL-literature, an important difference is in the role of learning. By design, RL-tasks emphasize the learning of an association of reward with a neutral stimulus. In economic experiments, because the reward parameters are presented directly – i.e. the magnitude and probability of outcomes – it is assumed that participants have already learned what this information means before entering the experiment. Given this assumption, our results suggest two different striatal signals. In most prediction-error models of learning, a prediction error can occur for two different reasons: 1) a reward was expected, but the magnitude was greater than expected; or 2) a reward occurred unexpectedly (i.e. the prior probability was low). Normally the weights in such models are adjusted by the prediction errors and will come to represent the expected value of the stimuli. Thus, a large weight might reflect a high value reward or one that is received frequently. For humans, it is likely that these two dimensions are processed, at least initially, as distinct entities. And so the existence of multiple prediction error signals seems plausible, similar to that found in primate striatum for separate classes of neurons that encode action-value and goal-value (Lau and Glimcher, 2008) or the dual-system model proposed by Daw et al. (2005). The existence of a separate prediction error for frequency of outcomes, without regard to magnitude, would also explain previous neuroimaging findings that implicate the striatum in signaling saliency (Cooper and Knutson, 2008; den Ouden et al., 2010; Horvitz, 2000; Schiffer and Schubotz, 2011; Wittman et al., 2008; Zink et al., 2003; Zink et al., 2004; Zink et al., 2006).

The existence of two prediction signals creates an obvious problem for the decision maker. Either the decision maker integrates them into an approximation of expected value, or they use one or the other. We found behavioral evidence for all three strategies. Some participants relied predominately on probability information to make their choices, some relied on magnitude information, and some used both (Fig. 4). Interestingly, the responsiveness of the ventral striatum to magnitude information was positively correlated with the behavioral propensity to rely on magnitude information (a negative correlation with  $PM_{diff}$ ). Thus, the striatal responses had behavioral manifestations, even before the second piece of information was presented. The dorsal striatum did not show this relationship, which suggests that all subjects processed probability information similarly, and that the behavioral differences were primarily a result

of how much weight they gave the magnitude information. There are, of course, many different forms for modeling how probability and magnitude information are integrated (Kahneman and Tversky, 1979; Prelec, 1998; Tversky and Kahneman, 1992; Wu and Gonzalez, 1996), but all make assumptions about the shape of these functions. We chose to model the behavioral effects of probability and magnitude by using an additive logistic model. Interestingly, we found that this additive form was as good as an EU-type form in modeling individuals' choices, but the additive form had the advantage that the coefficients obtained gave a direct readout of the relative weighting of probability and magnitude information. The  $PM_{diff}$  metric, however, may be interpreted in the context of EU; namely, a large positive  $PM_{diff}$  is behaviorally equivalent to a large concave curvature of the utility function (e.g. someone who is risk-averse), while a negative  $PM_{diff}$  is behaviorally equivalent to a convex utility function (someone who is risk-seeking). Thus, the correlation of the ventral striatal responsiveness with  $PM_{diff}$  could also reflect the individual risk preference, with greater responsiveness linked to risk-seeking. Finally, it has been suggested that the striatum encodes the variance of financial rewards (Christopoulos et al., 2009; Preuschoff et al., 2006). Although we did not specifically design our experiment to test this hypothesis, we note that the conditions of our experiment with larger magnitudes also had larger variances relative to the sure thing.

Decision under uncertainty is fundamentally a problem of divided attention. Two pieces of information – probability and magnitude – must be integrated to form an objective expectation of reward. Assuming that individuals can accurately process each dimension alone (a dubious assumption for probability), integrating the two is a complex cognitive operation. To perform this integration, the individual must attend to both elements, hold them in working memory, combine them, and compare the result to another option, also held in working memory. The observation of distinct signals for probability and magnitude is consistent with a second-order model of information integration (Shaw, 1982). In a second-order model, decision criteria are formed for each dimension of information and then the two criteria are integrated to form a response. For example, the agent would form a tentative response (gamble or sure-thing) based on probability and another tentative response based on magnitude. If the two responses are in agreement, then the choice process is complete. If the two types of responses differ, then the agent must choose one or the other to arrive at their actual choice. In contrast, a first-order model, which is implicit to expected utility theory, the decision maker integrates the two pieces of information and then applies a decision criterion to the result. For example, the agent would first multiply probability and magnitude (or some transformation of them), and if the result exceeded a threshold criterion, then they would choose the gamble. However, the non-overlapping representations of probability and magnitude information in the striatum are more consistent with the second-order model. Previous studies of basal ganglia connectivity have shown that the ventral striatum receives the majority of its inputs from the medial PFC and OFC, while the dorsal striatum receives inputs from the DLPFC (Draganski et al., 2008). In fact, the ventral striatal region we identified as being modulated by magnitude information spreads into the MPFC/OFC. At slightly lower thresholds of significance ( $P<0.005$ ), we also observe L DLPFC (-27, 24, 38) activity significantly modulated by probability information. Thus, the likely inputs for the two streams of information follow known fronto-striatal connectivity patterns.

Our results have implications for understanding the cognitive distortions that occur when individuals make decisions under uncertainty. Economic models, such as prospect theory, postulate a distortion of probability and/or magnitude information. Although the source of these distortions is not known exactly, perceptual processes are frequently implicated. In addition to perceptual distortions, our results suggest that the sequential processing of two dimensions of information, occurring in

distinct regions of the striatum, may result in a second-order decision process in which judgments are aggregated instead of information.

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## Appendix A. Supplementary data

Supplementary data to this article can be found online at [doi:10.1016/j.neuroimage.2011.11.008](https://doi.org/10.1016/j.neuroimage.2011.11.008).

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